Surface decoration of small coloured components [...]closely set into an adhesive ground.Mosaic pieces are usually small squares,triangles, or other regular shapes.

Encyclopedia Britannica















3D Ultrasound Mosaicing

DA - final Christian Wachinger

21 May 2007

Chair for Computer Aided Medical Procedures & Augmented Reality

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Clinical value of Mosaicing

- Spatial relationship among structures that are too large for a single volume is easier to understand – [Kim et al., '03]
- Sonographers have the flexibility to visualize anatomical structures from a variety of different angles – [Peetrons et al., '02] – [Leung et al., '05]
- Size and distance measurements of large organs are possible [Ying et al., '05]
- Individual structures within a broader context can be identified by having an image of the whole examination area – [Dietrich et al., '02]
- Specialists not used to ultrasound can better understand the spatial relationships of anatomical structures; helping to bridge the gap between the modalities and making it easier to convey sonographic findings to other experts – [Henrich et al., '03]

Concrete applications on the short run

- Breast Scanner
 - Flexible plate between body and transducer to ensure uniform deformation
 - No radiation exposure
 - "Matrix Scanning"
- DARPA Project
 - Cuff around the arm or leg
 - Direct treatment of internal bleedings on the battlefield by non-experts
 - "Cylindric Scanning"

YES, I DID HAVE MY MAMMOGRAM TODAY... WHY DO YOU ASK?

Agenda

- 1. Registration Strategies
- 2. Similarity Measures
- 3. Reconstruction
- 4. Experiments & Results
- 5. Conclusion & Further Development

Agenda

1. Registration Strategies

- 1. Problem statement
- 2. Pairwise Strategies
- 3. Simultaneous Strategies
- 2. Similarity Measures
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Mosaicing Framework

Problem statement

• In the literature proposed 3D mosaicing techniques by [Gee et al., '03] and [Poon et al., '06] use a sequence of pairwise registrations

→ High demands on the overlap invariance of similarity measures

Problem statement

Partial overlap: ill-conditioned registration

Problem statement

Accumulated Errors

Imaging Situations and Acquisition Graph

"Extended field-of-view"

Sequential Pairwise Registration

Intensity-based registration with bivariate similarity measures

$$(u_1) \xrightarrow{T_{1,2}} (u_2) \xrightarrow{T_{2,3}} (u_3) \xrightarrow{T_{3,4}} (u_4) \qquad T_k = \prod_{i=2}^k T_{i-1,i}$$

- **Problem:** Overlap dependence of similarity measures
 - 1. Usage of an ROI that is a subset of the overlap \Rightarrow But: Limited region of overlap further reduced
 - Penalize large spatial displacements
 ⇒ But: Manual adjustment to scenario

Complete Pairwise Registration

• Lie group normalization presented by Vercauteren et al. at MICCAI '06

Bases on the work of Xavier Pennec:

- Computing the mean of geometric features Application to the mean rotation, '98
- ^o Uniform distribution, distance and expectation problems for geometric features processing, '98
- Probabilities and Statistics on Riemannian Manifolds: Basic Tools for Geometric Measurements, '99
- ^a Intrinsic Statistics on Riemannian Manifolds: Basic Tools for Geometric Measurements, '06
- ^o Statistical Computing on Manifolds for Computational Anatomy, Habilitation, '06

Estimation problems on Lie groups

Distance between two points of a Lie group

 $dist(x,y) = dist(Id, x^{-1} \circ y)$ $= \left\| \log_{Id}(x^{-1} \circ y) \right\|$

- Exactly one Fréchet mean element exists
 $\mathcal{F}_x = \arg\min_{y \in \mathcal{G}} \left(\mathbb{E}[\operatorname{dist}(y, x)^2] \right)$
- The covariance matrix $\Sigma_{xx} = \mathbb{E}\left[\log_{\mathbb{E}[x]}(x) \cdot \log_{\mathbb{E}[x]}(x)^T\right]$

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Emphasizing pairs having high overlap with weights $\omega_{i,j}$

$$[\hat{T}_1, \dots, \hat{T}_n] = \min_{[T_1, \dots, T_n]} \sum_{(i,j)} \omega_{i,j} \cdot \mu_{\varepsilon}^2(\varepsilon_{i,j})$$

Registration with Lie group normalization

1. Start with initial global transformations $\mathcal{T} = \{T_1, \ldots, T_n\}$

2. Do

- 2.1 Deduce initial pairwise transformations $T_{i,j}$ from ${\mathcal T}$
- 2.2 Compute all pairwise registrations $T_{i,i}$
- 2.3 Estimate new \mathcal{T} from calculated $T_{i,j}$ with Lie normalization
- 3. While $(\varepsilon_t > \delta)$
- 4. Return ${\mathcal T}$

Agenda

- 1. Registration Strategies
 - 1. Problem statement
 - 2. Registration Scenarios
 - 3. Pairwise Strategies
 - 1. Sequential
 - 2. Complete

4. Simultaneous Strategies

- 1. Full-Simultaneous
- 2. Semi-Simultaneous
- 2. Similarity Measures
- 3. Reconstruction
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Simultaneous registration

- Registration of all n images at the same time
 - Direct optimization of the global transformations n*6 parameters
 - Considering the whole imaging setup multivariate similarity metrics
- Addressing the described problems
 - 1. Accumulation errors do not come up
 - 2. Better conditioned costfunction:
 - Overlap
 - Viewing angle dependence of US
- Increasing computational complexity
 - Higher dimensional parameter space
 - Evaluation of costfunction is more expensive

The compromise: Semi-Simultaneous Registration

- Optimizing only one transformation at a time
- **But** using a multivariate similarity measure

Do
For each i in
$$\{1, ..., n\}$$

Register u_i to $\{u_1, ..., u_{i-1}, u_{i+1}, ..., u_n\}$
for num steps by optimizing T_i
END
While alignment not satisfying

- Calculation of the Similarity Measure is faster
- Splitting up the high dimensional parameter space

Registration Strategies -Overview

	Sequential PW	Complete PW	Semi-Simultaneous	Full-Simultaneous
Optimization	6	6	6	n · 6
Similarity	Bivariate	Bivariate	Multivariate	Multivariate
Overlap	Sequence	All	All	All

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- 1. Registration Strategies
- 2. Similarity Measures
 - 1. Bivariate Measures
 - 2. Multivariate Extensions
 - 1. Summed-up bivariate extension
 - 2. Joint density function
 - 3. Voxel-wise extension
 - 3. Practical issues
- 3. Reconstruction
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Images as random variables

Pierre-Simon Laplace about probability theory:

"It is remarkable that a science which began with the consideration of games of chance should have become the most important object of human knowledge."

- Probability of one pixel to have the intensity i in the image
 - Image histogram has the role of the pdf
- Maximum Likelihood Estimation (MLE) Framework
 - Probability for the model m having the observations a

$$P(a = \{a_1, \dots, a_n\} | m) = \prod_{i=1}^n P(a_i | m)$$

Log likelihood function

 $\log \mathcal{L}(m|a) = \sum_{i=1}^{n} \log P(a_i|m)$

 $P(i) = \frac{N_i}{N}$

Imaging setup

$$u(x) = f(v(T(x))) + \varepsilon$$

u, v: images

- $\varepsilon:$ Gaussian noise
- f: intensity mapping

Probability function

$$P(u|v, T, \varepsilon, f) = P(\varepsilon = u(x) - f(v(T(x_k))))$$

Negative log-likelihood function

$$-\log \mathcal{L}(T,\varepsilon,f) = -\log P(u|v,T,\varepsilon,f)$$
$$= -\log P(\varepsilon = u(x) - f(v(T(x_k))))$$

Stationary white Gaussian noise

$$P(u|v,T,f,\sigma) = \frac{1}{\sqrt{2\pi\sigma}} e^{-\frac{1}{2}\frac{(u-f(v^{\downarrow}))^2}{\sigma^2}} \qquad \left[$$

 $v^{\downarrow} = v(T(.))$

Negative log-likelihood function

$$P(u|v,T,f,\sigma) = \frac{1}{\sqrt{2\pi\sigma}} e^{-\frac{1}{2}\frac{(u-f(v^{\downarrow}))^2}{\sigma^2}}$$

$$-\log \mathcal{L}(T, f, \sigma) = -\sum_{x_k \in \Omega_u} \log P(u(x_k) | v^{\downarrow}(x_k), f, \sigma)$$
$$= N \log \sqrt{2\pi} \sigma + \frac{1}{2} \sum_{x_k \in \Omega_u} \frac{(u(x_k) - f(v^{\downarrow}(x_k)))^2}{\sigma^2}$$

Assuming the identity as intensity map

$$-\log \mathcal{L}(T, f, \sigma) = N \log \sqrt{2\pi} \sigma + \frac{1}{2} \sum_{x_k \in \Omega_u} \frac{(u(x_k) - v^{\downarrow}(x_k))^2}{\sigma^2}$$

$$\propto \mathbb{E} \left[(u(x_k) - v^{\downarrow}(x_k))^2 \right]$$

➡ Sum of Squared Differences

- Intensity mapping that allows for an affine transformation $u \approx \alpha \cdot v + \beta$ \Rightarrow using normalized images $\tilde{u}(x) = \frac{u(x) \mathbb{E}[u(X)]}{\operatorname{Var}(u(X))}$
- Normalized Sum of Squared Differences

$$\begin{split} \text{NSSD}(T) &= & \mathbb{E}[(\tilde{v}(T(X)) - \tilde{u}(X))^2] \\ &= & \mathbb{E}[\tilde{v}^2(T(X)) - 2 \ \tilde{v}(T(X))\tilde{u}(X) + \tilde{u}^2(X))] \\ &= & \mathbb{E}[\tilde{v}^2(T(X))] - 2 \ \mathbb{E}[\tilde{v}(T(X))\tilde{u}(X)] + \mathbb{E}[\tilde{u}^2(X)] \\ &= & 1 - 2 \ \frac{\mathbb{E}[v(T(X))u(X)] - \mathbb{E}[v(T(X))]\mathbb{E}[u(X)]}{\text{Var}(v(T(X))) \ \text{Var}(u(X))} + 1 \\ &= & 2 - 2 \cdot \text{NCC}(v(T(X)), u(X)) \end{split}$$

Normalized Cross Correlation

- By further varying the assumptions for the intensity mapping f, Correlation Ratio (CR) and Mutual Information (MI) can be deduced
 - Paul A. Viola, "Alignment by Maximization of Mutual Information", '95
 - Roche et al., "Unifying Maximum Likelihood Approaches in Medical Image Registration", '00
 - Identity relationship: Sum of Squared Differences, Cross-Correlation
 - Affine relationship: Normalized Cross Correlation
 - Functional relationship: Correlation Ratio
 - Statistical relationship: Mutual Information

Extension of MLE to multiple images $u_1, \ldots, u_n : \text{images}$ $\varepsilon_1, \ldots, \varepsilon_n : \text{Gaussian noises}$

1. Summed-up bivariate extension

$$-\mathcal{L}(T) = -P(u_{1}^{\downarrow}|u_{2}^{\downarrow}, \dots, u_{n}^{\downarrow}, \vec{f}, \vec{\varepsilon})$$

$$= -P(\varepsilon_{2} = u_{1}^{\downarrow} - f_{2}(u_{2}^{\downarrow}), \varepsilon_{3} = u_{1}^{\downarrow} - f_{3}(u_{3}^{\downarrow}), \dots, \varepsilon_{n} = u_{1}^{\downarrow} - f_{n}(u_{n}^{\downarrow}))$$

$$= -\prod_{i=2}^{n} P(\varepsilon_{i} = u_{1}^{\downarrow} - f_{i}(u_{i}^{\downarrow}))$$

$$= -\prod_{i=2}^{n} \prod_{x_{k} \in \Omega} P(\varepsilon_{i} = u_{1}^{\downarrow}(x_{k}) - f_{i}(u_{i}^{\downarrow}(x_{k})))$$

$$-\log(\mathcal{L}(T)) = -\sum_{i=2}^{n} \sum_{x_{k} \in \Omega} \log P(\varepsilon_{i} = u_{1}^{\downarrow}(x_{k}) - f_{i}(u_{i}^{\downarrow}(x_{k})))$$

$$= -\sum_{i=2}^{n} \sum_{x_{k} \in \Omega} \log P(u_{1}^{\downarrow}|u_{i}^{\downarrow}, f_{i}, \varepsilon_{i})$$
Bivariate formula

Extension of MLE to multiple images

- Multivariate extensions by summing up the bivariate terms $\sum_{i=2}^{n} SM(u_1, u_i)$
- Corresponds to summing up the first line of the similarity matrix M

$$M^{\nabla} = \left(\begin{pmatrix} SM(u_1, u_2) & SM(u_1, u_3) & \cdots & SM(u_1, u_n) \\ SM(u_1, u_1) & SM(u_2, u_2) & u_3 \end{pmatrix} & \cdots & SM(u_1, u_n) \\ SM(u_2, u_1) & SM(u_2, u_2) & \cdots & SM(u_2, u_n) \\ \vdots & \vdots & \ddots & \vdots \\ SM(u_2, u_1) & SM(u_n, u_2) & \cdots & SM(u_n, u_n) \end{pmatrix} \right)$$

- □ Focus on one image ⇒ suits well for semi-simultaneous registration
- Full-simultaneous variant by summing up the matrix

$$\sum_{i < j}^{n} SM(u_i, u_j)$$

Interim summary -Multivariate Measures

	Pairwise	Semi-Simultaneous	Full-Simultaneous
SSD	$\mathbb{E}[(u - v^{\downarrow})^2]$	$\sum_{i=2}^{n} \omega_{1,i} \mathbb{E}[(u_1 - u_i^{\downarrow})^2]$	$\sum_{i < j} \omega_{i,j} \mathbb{E}[(u_i^{\downarrow} - u_j^{\downarrow})^2]$
NCC	$\mathbb{E}[\tilde{u}\cdot\tilde{v}^{\downarrow}]$	$\sum_{i=2}^{n} \omega_{1,i} \mathbb{E}[\tilde{u}_1 \cdot \tilde{u}_i^{\downarrow}]$	$\sum_{i < j} \omega_{i,j} \mathbb{E}[\tilde{u}_i^{\downarrow} \cdot \tilde{u}_j^{\downarrow}]$
CR	$\frac{\operatorname{Var}[\mathbb{E}(u v^{\downarrow})]}{\operatorname{Var}(u)}$	$\sum_{i=2}^{n} \omega_{1,i} \frac{\operatorname{Var}[\mathbb{E}(u_1 u_i^{\downarrow})]}{\operatorname{Var}(u_1)}$	$\sum_{i < j} \omega_{i,j} \frac{\operatorname{Var}[\mathbb{E}(u_i^{\downarrow} u_j^{\downarrow})]}{\operatorname{Var}(u_i^{\downarrow})}$
MI	$MI(u,v^{\downarrow})$	$\sum_{i=2}^{n} \omega_{1,i} \mathrm{MI}(u_1, u_i^{\downarrow})$	$\sum_{i < j} \omega_{i,j} \mathbf{MI}(u_i^{\downarrow}, u_j^{\downarrow})$

Extension of MLE to multiple images

2. Joint density function

$$-\log(\mathcal{L}(T)) = -\log P(u_1^{\downarrow}, u_2^{\downarrow}, \dots, u_n^{\downarrow})$$

=
$$-\sum_{x_k \in \Omega} \log P(u_1^{\downarrow}(x_k), u_2^{\downarrow}(x_k), \dots, u_n^{\downarrow}(x_k))$$

- Curse of dimensionality: Observations grow linearly, needed data for reliable estimation grows exponentially
- Not flexible to varying numbers of overlapping images
- \Rightarrow Not used for Mosaicing

Extension of MLE to multiple images

3. Voxel-wise extension

$$-\log(\mathcal{L}(T)) = -\log P(u_1^{\downarrow}, u_2^{\downarrow}, \dots, u_n^{\downarrow})$$

=
$$-\sum_{x_k \in \Omega} \log P^k(u_1^{\downarrow}(x_k), u_2^{\downarrow}(x_k), \dots, u_n^{\downarrow}(x_k))$$

- Independent but not identical distributed coordinate samples
- Allows for varying numbers of overlapping images
- Idea of pixel stack was introduced by Miller '02

Voxel-wise extension for SSD

$$\dots, f_n$$
: intensity mappings

$$-\log(\mathcal{L}(T)) = -\frac{1}{N} \sum_{x_k \in \Omega} \log P^k(u_1^{\downarrow}(x_k), \dots, u_n^{\downarrow}(x_k))$$

$$\approx -\frac{1}{N} \sum_{x_k \in \Omega} \log \prod_{i=1}^n P^k(u_i^{\downarrow}(x_k))$$

$$= -\frac{1}{N} \sum_{x_k \in \Omega} \sum_{i=1}^n \log \left(\frac{1}{\sqrt{2\pi\sigma}} e^{-\frac{1}{2} \frac{(f_i(u_i^{\downarrow}(x_k)) - \mu_k)^2}{\sigma_k^2}} \right)$$

$$= -\frac{1}{N} \sum_{x_k \in \Omega} \sum_{i=1}^n \left(\log \frac{1}{\sqrt{2\pi\sigma}} - \frac{1}{2} \frac{(f_i(u_i^{\downarrow}(x_k)) - \mu_k)^2}{\sigma_k^2} \right)$$

$$\approx \frac{1}{N} \sum_{x_k \in \Omega} \frac{1}{\sigma_k^2} \sum_{i=1}^n (f_i(u_i^{\downarrow}(x_k)) - \mu_k)^2$$

Voxel-wise extension for SSD

Assuming identity as intensity mapping

$$-\log(\mathcal{L}(T)) \approx \frac{1}{N} \sum_{x_k \in \Omega} \frac{1}{\sigma_k^2} \sum_{i=1}^n (u_i^{\downarrow}(x_k) - \mu_k)^2$$

Sum of voxel-wise variances (SVV)

$$\begin{aligned} \text{SVV}(u_1, \dots, u_n) &= \frac{1}{N} \sum_{x_k \in \Omega} \frac{1}{m_k} \sum_{i=1}^{m_k} (u_{\iota(i)}^{\downarrow}(x_k) - \mu_k)^2 \\ &\approx \sum_{x_k \in \Omega} \omega_k \cdot \mathbb{E}_i \left[(u_{\iota(i)}^{\downarrow}(x_k) - \mu_k)^2 \right] \\ \mu_k &= \frac{1}{m_k} \sum_{i=1}^{m_k} u_{\iota(i)}^{\downarrow}(x_k). \end{aligned} \qquad \begin{aligned} &\frac{m_k : \text{overlapping images at } x_k}{u : \{1, \dots, m_k\} \to \{1, \dots, n\}} \\ &\omega_k : \text{weighting coefficient} \end{aligned}$$

Voxel-wise extension for MI

• Congealing [Lilla Zöllei '06, Miller '02]

$$\log(\mathcal{L}(T)) = \frac{1}{N} \sum_{x_k \in \Omega} \log P^k(u_1^{\downarrow}(x_k), \dots, u_n^{\downarrow}(x_k))$$
$$\approx \frac{1}{N} \sum_{x_k \in \Omega} \log \prod_{i=1}^n P^k(u_i^{\downarrow}(x_k))$$
$$= \frac{1}{N} \sum_{x_k \in \Omega} \sum_{i=1}^n \log P^k(u_i^{\downarrow}(x_k))$$
$$\approx \sum_{x_k \in \Omega} \omega_k \cdot \mathrm{H}(P^k)$$

Summary - Multivariate Similarity Measures

	Pairwise	Semi-Simultaneous	Full-Simultaneous	Voxel-Wise
SSD	$\mathbb{E}[(u - v^{\downarrow})^2]$	$\sum_{i=2}^{n} \omega_{1,i} \mathbb{E}[(u_1 - u_i^{\downarrow})^2]$	$\sum_{i < j} \omega_{i,j} \mathbb{E}[(u_i^{\downarrow} - u_j^{\downarrow})^2$	$\sum_{x_k \in \Omega} \omega_k \mathbb{E}_i[(\mu_k - u_i^{\downarrow}(x_k))^2]$
NCC	$\mathbb{E}[ilde{u}\cdot ilde{v}^{\downarrow}]$	$\sum_{i=2}^{n} \omega_{1,i} \mathbb{E}[\tilde{u}_1 \cdot \tilde{u}_i^{\downarrow}]$	$\sum_{i < j} \omega_{i,j} \mathbb{E}[\tilde{u}_i^{\downarrow} \cdot \tilde{u}_j^{\downarrow}]$	$\sum_{x_k \in \Omega} (\omega_k \cdot \tilde{u}_1^{\downarrow} \cdot \tilde{u}_2^{\downarrow} \cdots \tilde{u}_n^{\downarrow})$
CR	$\frac{\operatorname{Var}[\mathbb{E}(u v^{\downarrow})]}{\operatorname{Var}(u)}$	$\sum_{i=2}^{n} \omega_{1,i} \frac{\operatorname{Var}[\mathbb{E}(u_1 u_i^{\downarrow})]}{\operatorname{Var}(u_1)}$	$\sum_{i < j} \omega_{i,j} \frac{\operatorname{Var}[\mathbb{E}(u_i^{\downarrow} u_j^{\downarrow})]}{\operatorname{Var}(u_i^{\downarrow})}$	_
MI	$\operatorname{MI}(u,v^{\downarrow})$	$\sum_{i=2}^{n} \omega_{1,i} \mathrm{MI}(u_1, u_i^{\downarrow})$	$\sum_{i < j} \omega_{i,j} \mathrm{MI}(u_i^{\downarrow}, u_j^{\downarrow})$	$\sum_{x_k\in\Omega}\omega_k\mathbf{H}(P^k)$

Practical Issues

- Normalization of transformations \rightarrow no sliding
- Speeding up the process
 - Region of overlap (ROO)
 - Semi-simultaneous approach with partial compounding
 - Stochastic Similarity Measures

Stochastic Similarity Measures

- Taking samples of the similarity of images only at random locations
- □ [Zöllei '06] used 0.05% 2.5%
- Enormous speed-up
- Fine-grained stochastic pyramids good complement to coarse-grained Gaussian pyramid

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 $X_k = \{x_k^1, \dots, x_k^m\}$

General compounding methods

- 1. Selection: $\operatorname{Sel}_k^j = x_k^j$
- 2. Mean: Mean_k = $\mathbb{E}[X_k]$
- 3. Median: Median_k = $median\{x_k^1, \dots, x_k^m\}$
- 4. Max: $\operatorname{Max}_k = \max\{x_k^1, \dots, x_k^m\}$
- 5. Min: $\operatorname{Min}_k = \min\{x_k^1, \dots, x_k^m\}$
- 6. Geometric Mean:

Geometric Mean_k =
$$\sqrt[n]{x_k^1 \cdot x_k^2 \cdots x_k^m}$$

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Eile Vi

Scanline

Registration

ROI Eroc 0 maxiter 1000 Downs 1 ♦ 1 Lie Optim Best Net Y -0.0 Z 1.9 St

Mosaicing prototype for exneriments

rasound Stitching			
w <u>P</u> ose <u>H</u> elp			
2D Pairs for Registration ✓ 0 <-> 1 1 <-> 2 2 <-> 3 ✓ All Show Pair Reg Pair			
Res Fusion Window selected volume			
on Visualization Advanced			
n Strategy leq Simultaneous II PW / Sim Measure Optimization € Best Neighbor €	Volume Fusion Window		
Inside Min. Ran % Step Size -1 100 10.0 maxeval partol. fun.tol. 12000 0.01 0.0001 ampling: Init Init	Transversal	Coronal	
Reg Cycles Norm tion Rotation 0 Type 0.00 Reset 0 Bound Box 0 Inter			K
1)	64	64)	
	Fading (

US specific image preprocessing

- Speckle noise reduction
 - Low-pass filtering
- Shadow suppression
 - Shadow has negative influence on registration and compounding

Clay spine

Similarity plot:

Clay vessel

Pairwise

Lie normalization

0

Semi-Simultaneous

Full-Simultaneous

Abdominal phantom - with optical tracking

$$T_{1,2} T_c = T_c T_2 T_1^{-1}$$
$$A \cdot X = X \cdot B$$

Random study on abdominal phantom

- 8 images
- Up to ± 20 mm/degree random initial displacement
- 100 registrations
- Sum of Squared Differences
- Plotting mean and standard deviation

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Conclusion

- Ultrasound mosaicing as multiple image alignment
- Proposal of specific registration strategies for mosaicing
- Deduction of multivariate extensions for similarity measures under usage of a maximum likelihood framework
- Experiments show the superior performance of proposed strategies

Further Development

- Integrating phase information
- Model-based registration
- Stochastic optimization
- Non-rigid registration
- Parallelization

Grau et al., Miccai '05 & '06

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The End